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# INTRODUCTION

#### **Background**

Brain-computer interfaces (BCIs) enable users to communicate or control devices by translating brain signals into commands, bypassing the motor system. The code-modulated visual evoked potential (c-VEP) BCI is one of world's fastest non-invasive BCI systems<sup>[1]</sup>.

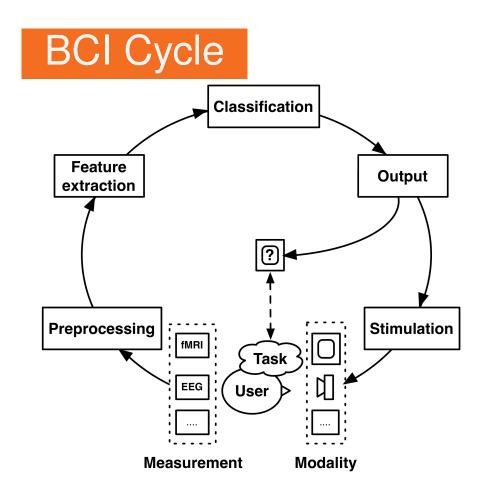
#### The Problem

Most BCIs are gaze-dependent: They require users to move their eyes to a target location. This excludes users with impaired oculomotor function.

#### This study

We present the first demonstration of a gaze-independent c-VEP BCI. We evaluated three parallel, simultaneous wellknown gaze-dependent (overt) BCI paradigms, here in a gaze-independent (covert) way:

- ▶ P300 ERP the response to an infrequent target
- ► Alpha the lateralisation of alpha (10 Hz) bandpower
- > c-VEP the response to pseudo-random visual stimulation



Adapted from [2]

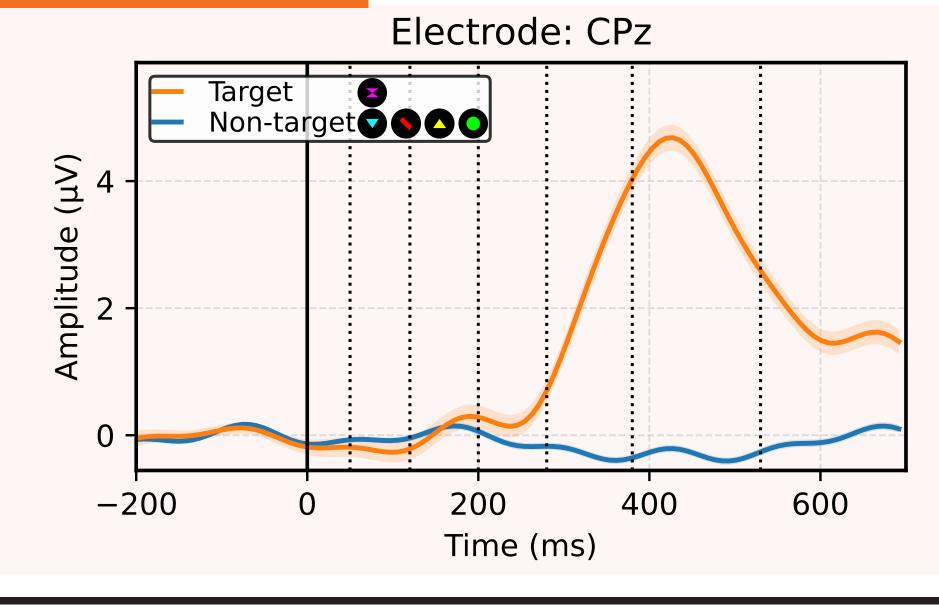
# Covert vs Overt

## METHODS

#### P300 ERP DECODING WITH BT-LDA -

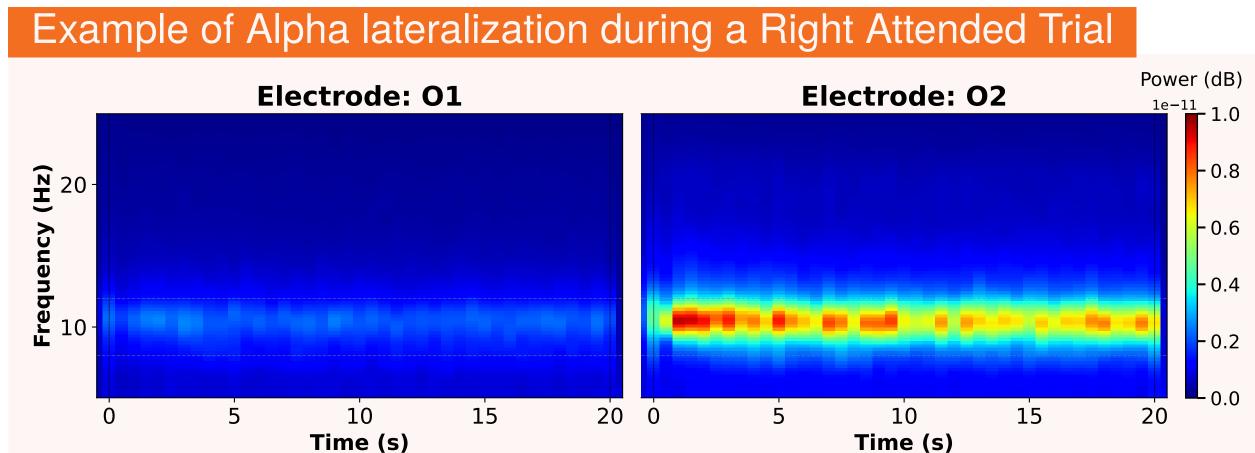
We used a state-of-the-art P300 ERP decoding pipeline that included block-Toeplitz linear discriminant analysis (BT-LDA)<sup>[3]</sup> to classify target from non-target epochs. Epoch classification was integrated over time using Pearson's correlation to classify left from right attended trials.

#### Example of the P300 ERP



# ALPHA DECODING WITH CSP AND S-LDA

We used a state-of-the-art 10 Hz visual alpha-lateralization decoding pipeline [4] that included common spatial patterns (CSP) and shrinkage linear discriminant analysis (s-LDA) to classify left from right attended trials.

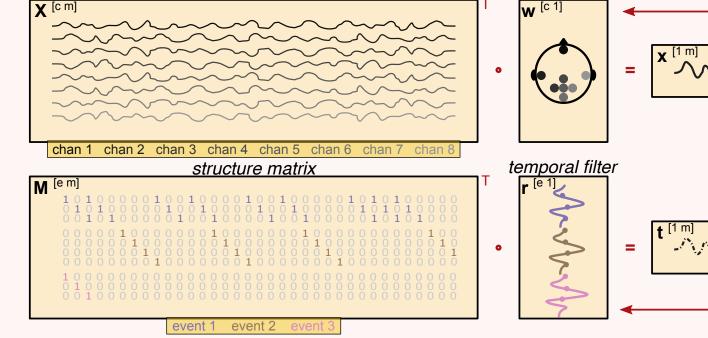


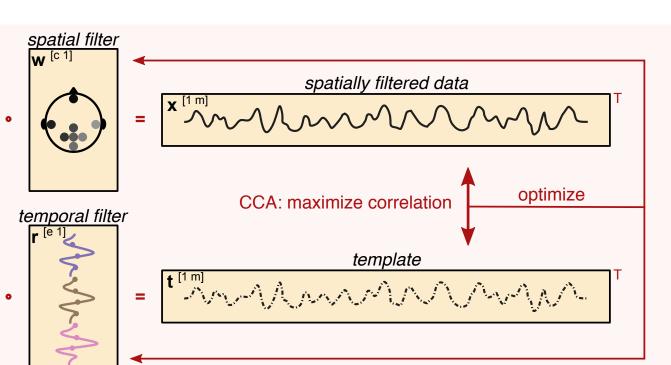
# C-VEP DECODING WITH CCA -

Time (s)

We used a state-of-the-art c-VEP decoding pipeline that included reconvolution canonical **correlation analysis (rCCA)** to classify left from right attended trials<sup>[5]</sup>.

# Reconvolution CCA

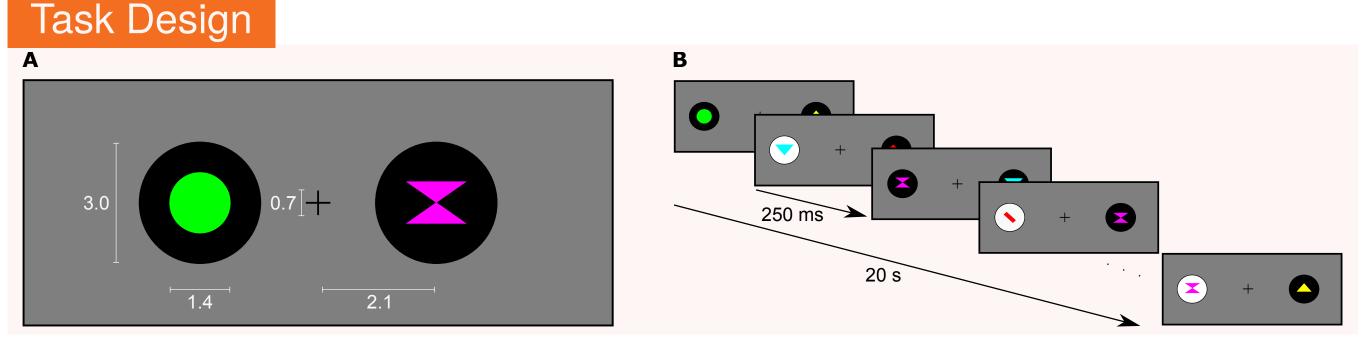




# **EVALUATION**

Decoding pipelines were evaluated with 4-fold chronological cross-validation. We derived decoding curves by incrementally extending each trial's decision window (1.25 s steps to 20 s) and computing classification accuracy at each step. Each pipeline was evaluated both with (w/) and without (w/o) independent component analysis (ICA)-based artifact removal.

# **EXPERIMENT**



#### **Participants:** 29 healthy adults

#### Task (per trial)

- 1. Fixate the center fixation cross; no eye movements.
- 2. Covertly attend cued side (left/right); ignore the other.
- 3. Count hourglasses (targets) on the attended side only.

## Stimulus protocol $\rightarrow$ Neural features

Foreground shape stream (5 shapes; 1 target)  $\rightarrow$  P300 ERP

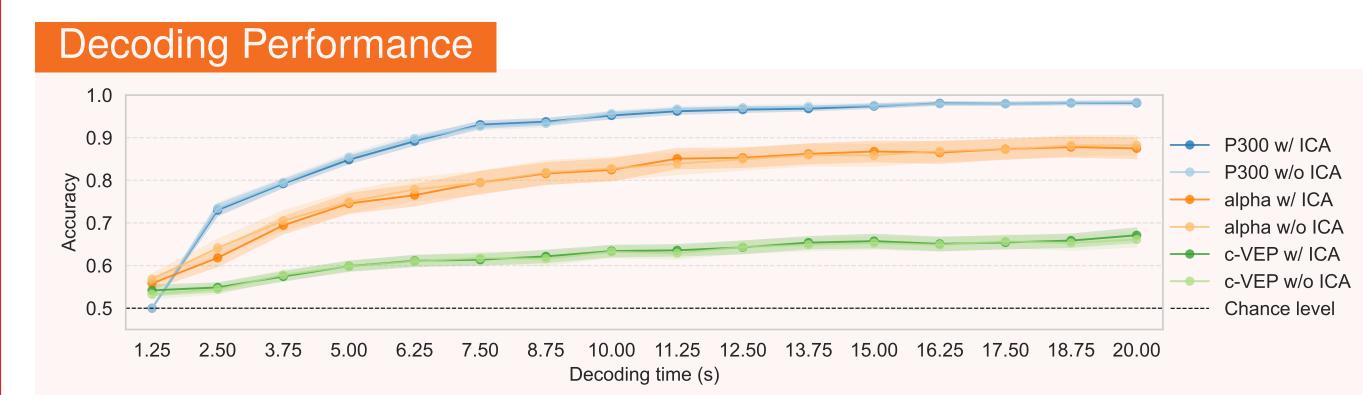
Background random black/white flickers  $\rightarrow$  *c-VEP* 

Covert spatial attention (left/right) → Alpha lateralization

# Key EEG Electrodes P300 Alpha & c-VEP

7.5

# RESULTS



- Accuracy of P300 > alpha > c-VEP
- Accuracy increases over decoding time
- No difference in accuracy between w/ ICA and w/o ICA

#### Which method achieves the best accuracy over time?

Table 1. Mean classification accuracy (%) at each time interval w/ and w/o ICA. Time (s) c-VEP w/ ICA c-VEP w/o ICA alpha w/ ICA alpha w/o ICA P300 w/ ICA P300 w/o ICA

			1	I		
 5.0	59.9	59.8	74.6	75.0	84.8	85.4
10.0	63.4	63.2	82.5	82.8	95.2	95.6
15.0	65.7	65.3	86.8	85.9	97.4	97.6
20.0	67.1	66.1	87.5	88.2	98.1	98.3

# When does each method reach key accuracy thresholds?

Table 2. Time (s) at which the mean accuracy reaches a threshold w/ and w/o ICA Accuracy (%) | c-VEP w/ ICA | c-VEP w/o ICA | alpha w/ ICA | alpha w/o ICA | P300 w/ ICA | P300 w/o ICA 60.0 70.0 5.0 80.0

# **DISCUSSION** -

90.0

# Our findings suggest:

- the feasibility of gaze-independent c-VEP BCI
- the **competitiveness** of c-VEP with SSVEP<sup>[6]</sup>
- a weak attentional modulation for c-VEP during parallel stimulation [7]
- that the results are not caused by fixational eye movements
- the high performance of **sophisticated decoding** pipelines

# TAKE-AWAY

We showed for the first time the feasibility of a gaze-independent c-VEP BCI.

# OPEN QUESTIONS -

- Can we improve performance by combining ERP, alpha and c-VEP into a **hybrid decoding**?
- Can we improve c-VEP by **optimizing stimulation** parameters like size, distance, etc.?
- How well do the presented results generalize from a healthy to a **patient population**?
- Can we extend these results from 2 classes to **more classes**?
- Can we use **dynamic stopping**<sup>[8]</sup> to shorten stimulus presentation?

# REFERENCES

- [1] Martinez-Cagigal et al. (2021) J Neural Eng doi:10.1088/1741-2552/ac38cf
- [2] Van Gerven et al. (2009) *J Neural Eng* doi:10.1088/1741-2560/6/4/041001
- [3] Blankertz et al. (2008) IEEE Sig. Proc. Mag. doi:10.1109/MSP.2008.4408441
- [4] Sosulski & Tangermann (2022) *J Neural Eng* doi:10.1088/1741-2552/ac9c98
- [5] Thielen et al. (2021) *J Neural Eng* doi:10.1088/1741-2552/abecef [6] Egan et al. (2017) *J Neural Eng* doi:10.1088/1741-2552/aa6bb2
- [7] Narayanan et al. (2024) *Proc. Graz BCI Conf.* doi:10.3217/978-3-99161-014-4-060
- [8] Ahmadi et al. (2024) Frontiers in Human Neuroscience. doi:10.3389/fnhum.2024.1437965



Code is available at: https://github.com/rvodila/covert\_cVEP\_2025.

Lab: https://neurotechlab.socsci.ru.nl/